

Identification of paediatric tuberculosis from airway shape features

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Introduction

- Prevalence of TB is still high, particularly in developing countries
- Poor detection rates in children
- Primary TB in children is characterised by lymphadenopathy - leading to displacement and stenosis of airway branches

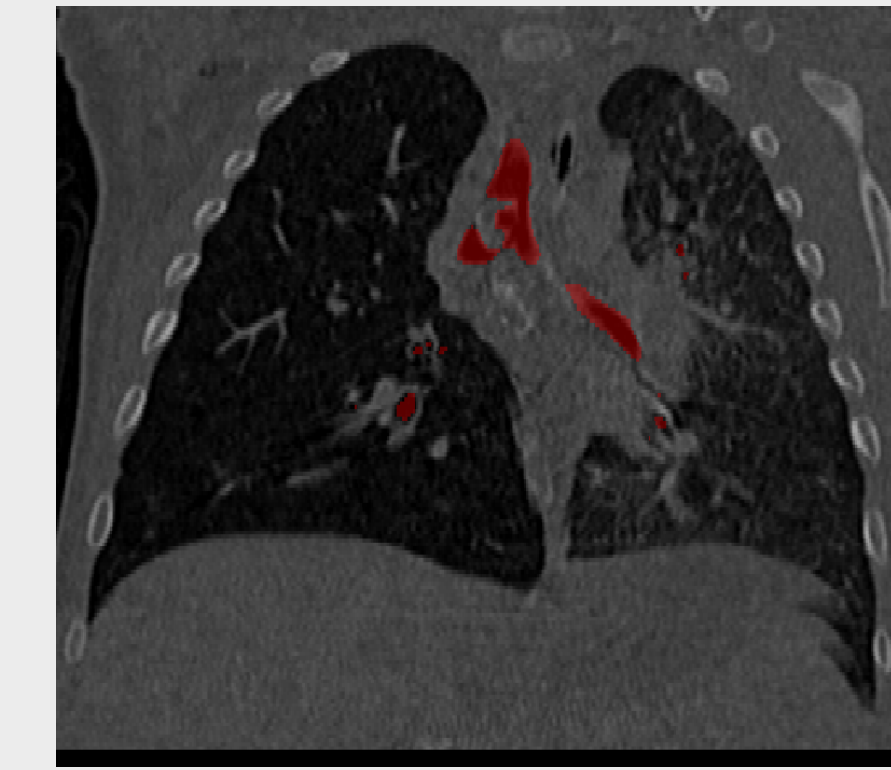
Aim: Assist in the detection of TB from airway shape
Segment and model airway shape changes from CT scans



Method

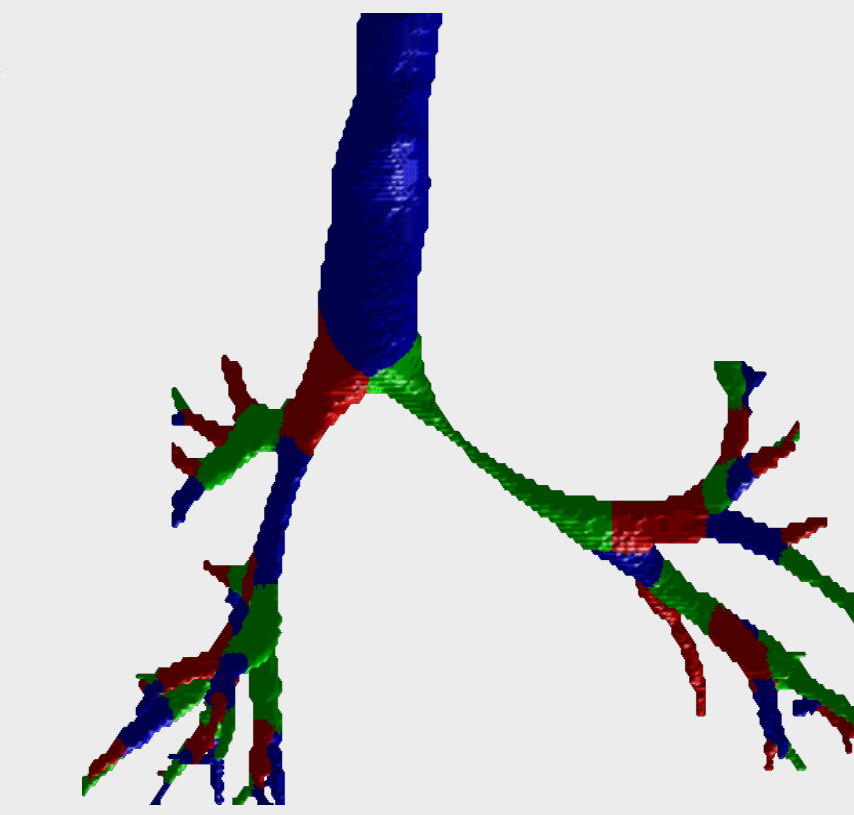
Airway Segmentation

- Detect trachea
- 3D morphological closing and reconstruction
- Seeded region growing



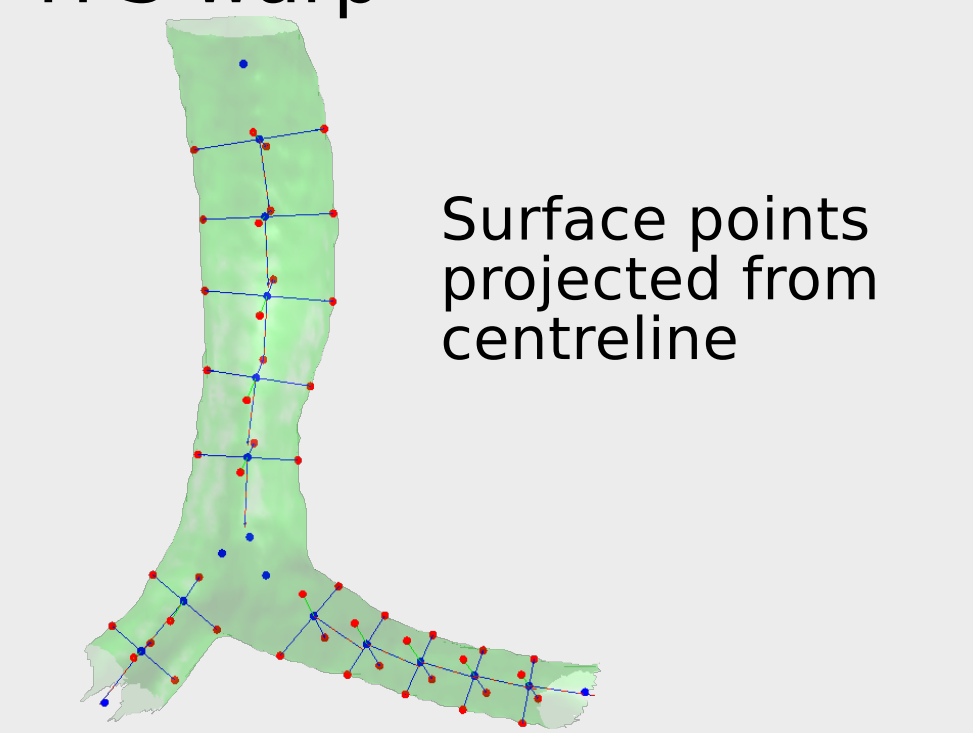
Skeletonisation and branch point detection

- Iterative topology preserving thinning
- Branch point detection by voxel connectivity



Airway Correspondence

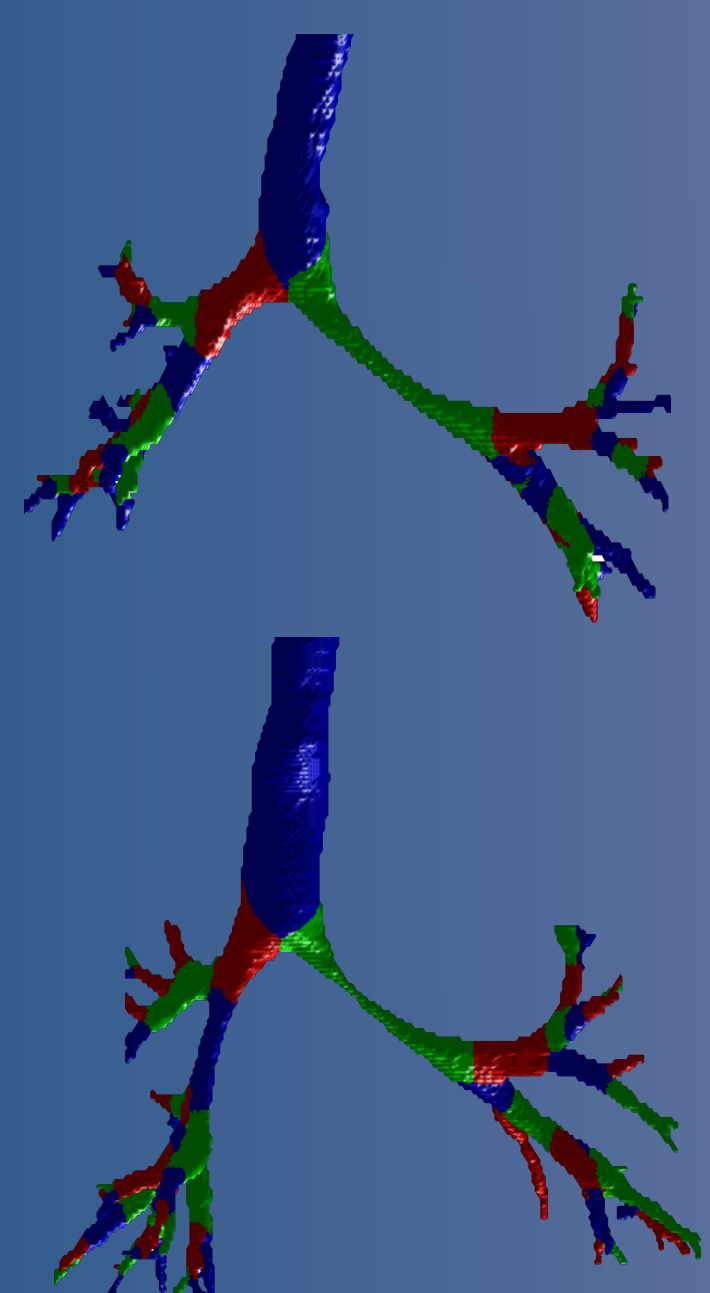
- Equidistant sampling of centreline
- Projection of points onto surface orthogonal to centreline
- Surface points used as landmark points for TPS warp



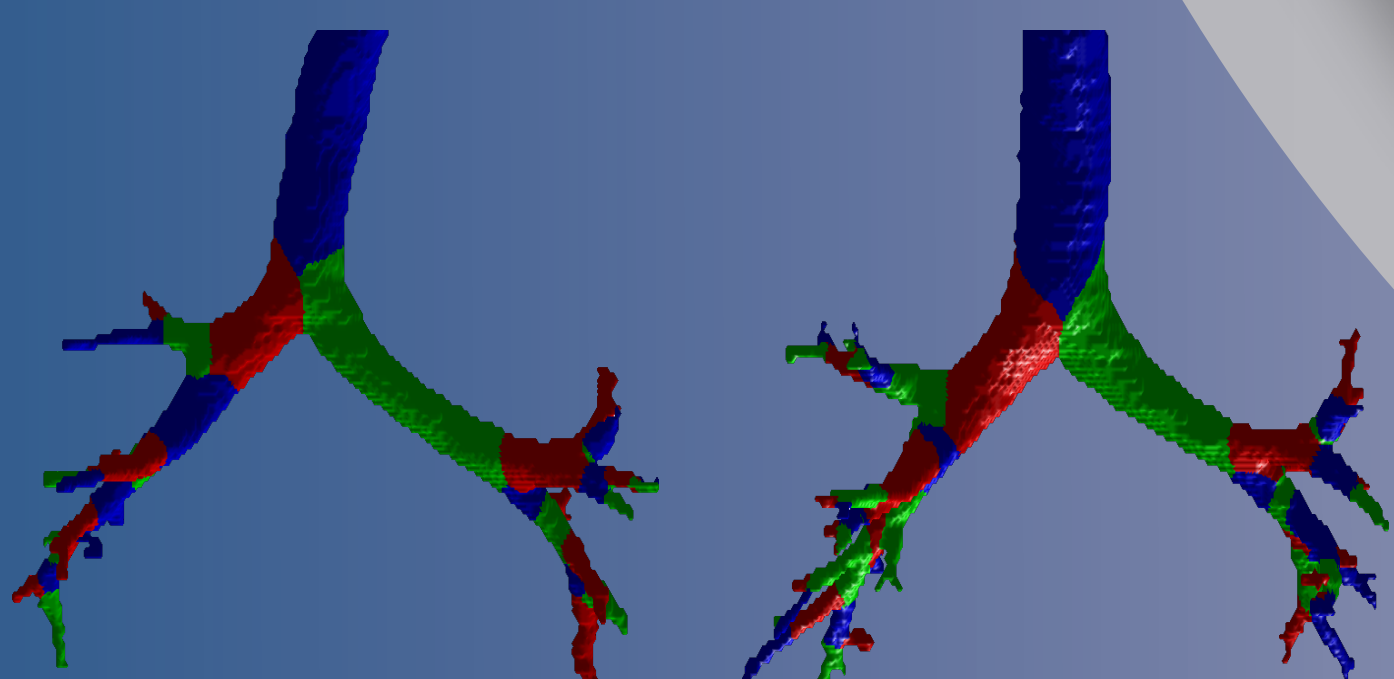
Dataset

- 61 Patients
 - TB and non-TB
 - Mean 33 months
 - Min 2 months
- CT Scan
 - Axial plane 0.3-0.5mm
 - Slice thickness 0.7-1mm

Airways of TB patients with narrowing in left main bronchus and bronchus intermedius:



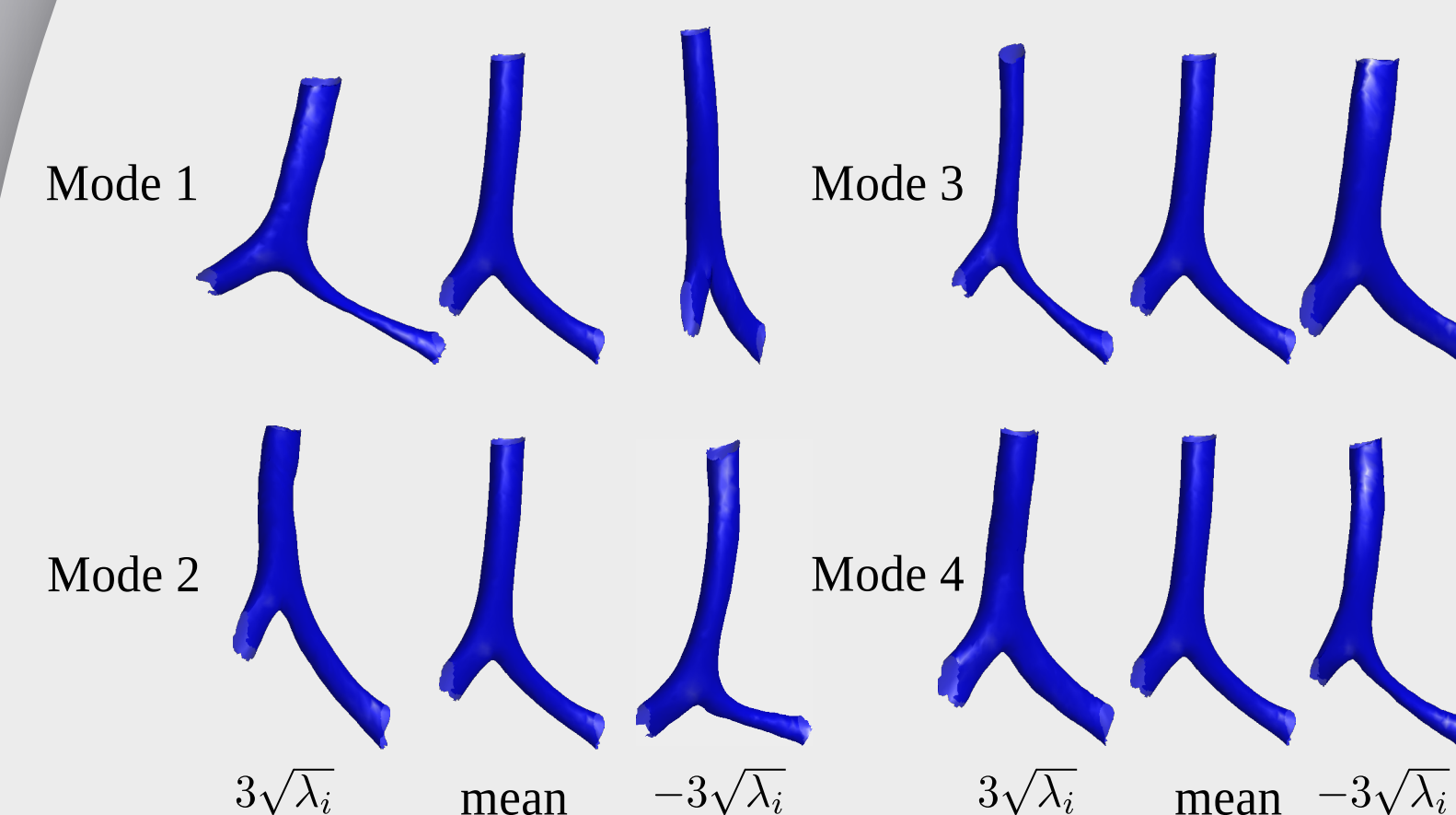
Airways of non-TB patients:



Method 1: PCA Features

- 3n input vector where n is the number of vertices
- Projection onto orthogonal components to generate features

Airway variation along the first 4 modes



Method 2: Branch Features

- Alternative set of features:
- ratio of orthogonal diameters
 - ratio of local minima and maxima
 - branch length and diameter
 - carinal angle

Local Alignment

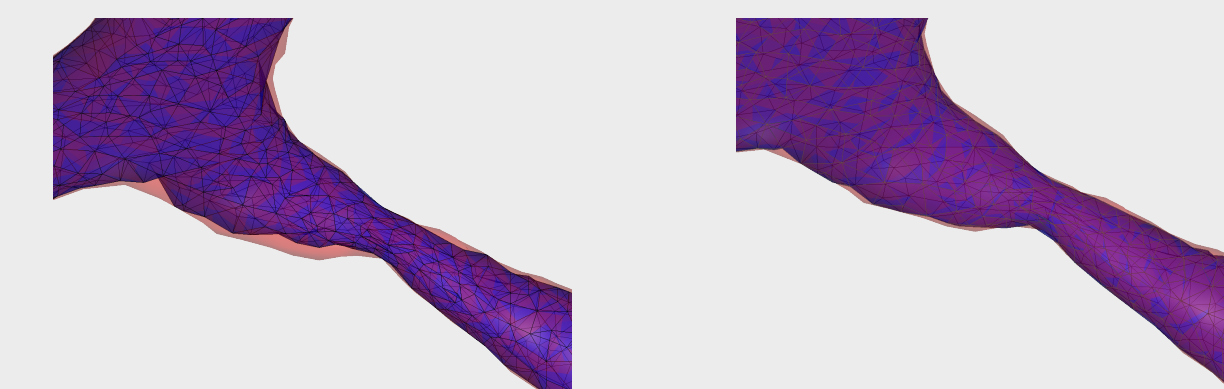
- Local alignment of surface required after TPS
- Forcing function directs alignment
- Expansion/contraction force improves matching with stenosed branches

$$F_{i,1} = \vec{r}_i - \vec{t}_i \quad \text{Closest point}$$

$$F_{i,2} = \sum_j^p \hat{v}_j (|\vec{v}_j| - |\vec{v}_0|) \quad \text{where } \vec{v}_j = \vec{t}_j - \vec{t}_i \quad \text{Mesh preserving term}$$

$$F_{i,3} = \hat{n}_i (\hat{n}_i \cdot F_{i,1}) \quad \text{Expansion/contraction force}$$

$$F_{i,tot} = \alpha F_{i,1} + \beta F_{i,2} + \gamma F_{i,3}$$



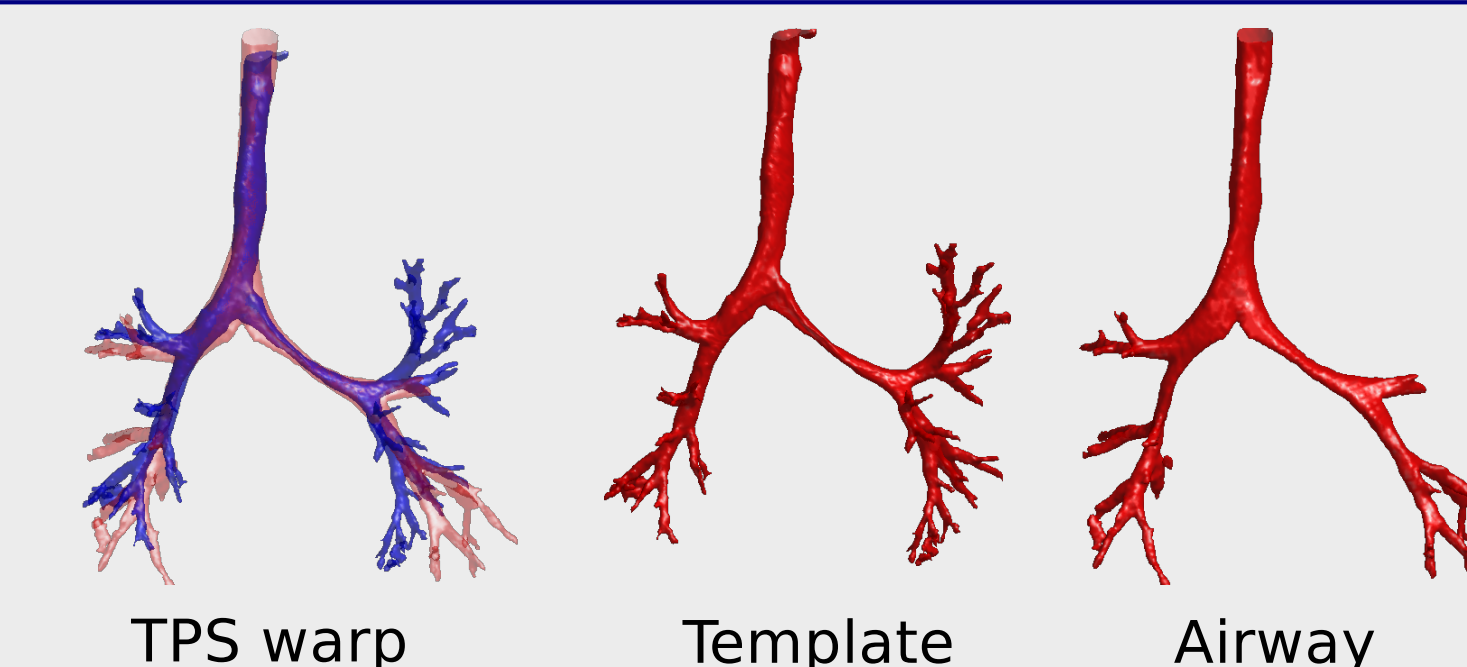
Closest point matching (F1+F2) Improvement using expansion/contraction force (F1+F2+F3)

Thin plate spline warp

- Warp vertices onto a template airway to generate matching vertices
- Landmark points direct warp by minimisation of bending energy
- ~1500 vertices

$$f_j(P_j) = \sum_{i=1}^k w_{ij} U(P_j - P_{ij}) + a_0 + a_x x + a_y y + a_z z$$

Landmark points match exactly. Other points interpolate landmark points. Weighting factors found from landmark points on template and airway.



Classification

- Classification to compare two feature vectors:
 - 10 PCA modes
 - 90% of airway variation
 - 10 radius based features
- Support vector machines
- Parameter selection and validation using nested leave-one-out cross validation

Results

- Detection of paediatric TB cases from airway shape

	Sensitivity	Specificity
PCA feat	86%	91%
Branch feat	86%	94%

Conclusions

- Both PCA based features and branch features accurately distinguish between TB and non-TB cases
- This method shows the potential of airway shape analysis to assist in the detection of airway pathology
- Future work:
 - Test method on a larger dataset
 - Local analysis of pathology

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